Abstract

In a single case longitudinal study, a 70 year old female subject who has had a subcortical stroke 8 years prior, was tested three times in fMRI using an interactive MRI-compatible VR environment. The subject performed sequential finger movements with her right (unaffected) hand. Her hand motion (recorded with the data glove) animated either the ipsilateral (corresponding) or contralateral (mirrored) virtual hand model. In a visual feedback control condition, the virtual hand models were replaced with ellipsoids. In between the second and third session, the patient participated in an intensive, two-week long VR-based training of her affected upper extremity. When comparing activation in the mirrored versus the non-mirrored virtual visual feedback condition, no significant activation was noted in motor or premotor areas in the baseline 1 or baseline 2 sessions. However, increased activation in the ipsilesional motor cortex occurred as a result of training, despite the absence of active involvement of the ipsilesional motor cortex in this condition. The left motor cortex was also recruited in this condition (though weaker) despite the subtracted out ellipsoid condition (in which subjects also moved their hand). Thus, the contralateral (mirrored) visual feedback may have had a facilitory effect bilaterally. These findings might have some important implications for the development of novel therapies in the acute phase, when paresis and the potential for neural remapping are greatest.

I. Introduction

Impaired force generation in the fingers and hand (paresis) occurs in 70–85% of individuals who have had a stroke [1,2]. Paresis is characterized by reduced strength and diminished or absent motor evoked potentials (MEP), and can occur even due to partial damage of the corticospinal tract (CST) system [3–6]. The prognosis to recover from paresis is higher for patients in whom MEPs can be elicited in the few weeks after stroke [5,7] and for individuals in whom cortical activation (measured with functional MRI, fMRI) shifts from the contralesional hemisphere (that often over-compensates after a stroke) to the ipsilesional hemisphere [8,9], [10–12]. Thus, empirical data suggest that recovery is dependent on entraining the intact ipsilesional CST system to assume the functions of the lesioned areas; a process of remapping functions onto new circuits.

This paper presents preliminary data that demonstrate that training a patient who is in the chronic phase after stroke on a set of virtual reality (VR)-based training exercises may bolster the remapping of ipsilesional motor cortex. For this, the patient trained for 2 weeks (10 sessions)
on a battery of hand and arm tasks embedded in a VR environment. To assess cortical remapping, the patient participated in three fMRI sessions. The first two baseline sessions were separated by 6 months of no therapy and controlled for effects due to spontaneous recovery. The last session occurred after the training protocol. During the fMRI session, the subject performed sequential finger movements with the unaffected right hand which actuated either a left or a right virtual hand model. During these blocks, the affected hand remained motionless. Additional control blocks in which the virtual hand models were replaced by obliquely rotating ellipsoids controlled for non-specific activation. We hypothesized that time-locking movement of the unaffected hand (involving the contralesional hemisphere) with the opposite virtual hand would collide an interhemispherically transferred motor program with high-fidelity visual feedback in the ipsilesional motor cortex. Thus, if remapping in the ipsilesional motor cortex occurred as a result of training, it should manifest as increased activation despite the absence of active involvement of the ipsilesional motor cortex in this condition.

II. METHODS

A. Subject

A right-handed [13], 70 year old female subject participated after signing informed consent approved by the IRB Committees of NYU and NJIT. The subject sustained a right hemispheric subcortical stroke in 2000. Her medical presentation is significant for hypertension which is controlled medically and asthma. She presents with mild left side hemiparesis resulting in a Chedoke-McMaster Impairment Inventory stage of 7 for the arm, 4 for her hand, 6 for the leg and 4 for her foot. She presents with 1/4 spasticity of her finger flexors and plantar flexors. She ambulates in the community without an assistive device or orthosis. She is independent in all basic and instrumental activities of daily living without adaptive equipment, and is the primary home-maker for her family.

B. Task

The subject performed sequential finger movements with her right (unaffected) or left (affected) hand. Her hand motion (recorded with the data glove) animated either the ipsilateral (corresponding) or contralateral (mirrored) virtual hand model (Fig 1). Two visual feedback control conditions were also added. In these conditions, the virtual hand models were replaced with ellipsoids that rotated about an oblique axis at a rate of 1 Hz (a comparable rate to the subject’s finger movement). The non-anthropomorphic ellipsoids controlled for non-specific visual effects related to size, color, object movement, location of the object in the visual field, and eye movement. Four functional fMRI runs were performed with the subject using the left hand, and four with the right hand. The visual feedback conditions were interleaved within each run (10 trials per condition). The inter-trial interval was randomly varied between 3–7 seconds to introduce temporal jitter into the fMRI acquisition.

C. The Virtual Reality System

The setup has been described elsewhere [14]. Briefly, hand kinematics were collected with an MRI-compatible left- and MRI-compatible right hand 5DT Data Glove 16 MRI (Fifth Dimension Technologies, 5DT Data Glove 16 MRI, http://www.5dt.com) that was interfaced with the virtual environment (developed with Virtools and VRPack plugin that communicated with the open source VRPN (Virtual Reality Peripheral Network, [15]). The data gloves use fiber optics to measure each metacarpophalangeal [16] joint, proximal interphalangeal (PIP) joint, and finger abduction angles. In the technician’s room, the fiber optic signals are digitized and connected to the serial port of a PC running the simulation. The VR simulation was projected through a rear-view display and subjects viewed it through a rear-facing mirror. Prior to the experiment, the data gloves were calibrated to each hand and the subject verified that the quality of her movement corresponded to that of the virtual hand models. The onset of the
virtual simulation and of the data glove acquisition was triggered by back-tic TTL transmitted from the scanner.

**D. FMRI Data Acquisition and Preprocessing**

Magnetic resonance imaging was performed using a 3-T Siemens Allegra head-only scanner with a Siemens standard head coil. T1-weighted structural (TR=2500ms, TE=3.93ms, FOV=256mm, Flip angle=8°, thickness=1mm, voxel size=1×1×1mm, resolution=256) and functional images (TR=2500ms, TE=30ms, FOV=192mm, flip angle=85°, voxel size=3×3×3mm, resolution=64, bandwidth=4112 Hz/px, echo-spacing=0.31ms, 46 slices, thickness=3mm, number of volumes=120) Two dummy images were acquired (but not saved) at the start of each run to account for field inhomogeneity. FMRI data were preprocessed and analyzed with SPM5. Images were realigned, co-registered, and spatially normalized to the Montreal Neurological Institute template, and smoothed (8mm kernel).

**E. FMRI Analysis**

Our first effect of interest was whether visual feedback of the virtual hand model corresponding to the affected side but actuated by the motion of the subject’s unaffected hand (contralateral visual feedback condition) would lead to increased activation in the motor cortex ipsilateral to the behaving hand (i.e. the non-acting ipsilesional hemisphere) (see Fig. 1). For this effect, we compared activation when the subject performed the task with her right (unaffected) hand but received real time feedback of her movement through the contralateral (left) virtual hand which corresponded to her affected side with the same condition but when the virtual hand models were replaced by the moving ellipsoids. Thus, everything was identical in both conditions except the viewed virtual object. Our second effect of interest was whether the above effect would be facilitated by having the subject train her affected hand and arm in a VR environment for 2 weeks. Thus, we repeated the fMRI experiment three times. The first and second sessions (baseline 1 and baseline 2) were separated by 6 months of no training to establish an absence of spontaneous neural changes. The second and third sessions (baseline 2 and post-test) were separated by 2 weeks of intense training on a different set of tasks in VR. Given the limited power in our preliminary data and to maximize the chances of observing even slight changes in activation, we used a liberal threshold of p<0.05 and a minimum extent of 10 voxels.

**F. Description of VR-Based Training**

The sensorimotor training of the hemiparetic upper extremity used a novel robotic system NJIT-RAVR,[17] with haptic effects and objects presented in three-dimensional VR environments. This system was used to train the hand and arm together as an integrated functional unit for 2–3 hour sessions for eight days. The training utilized four interactive VR environments that have been developed previously[18] Tracking of the arm endpoint in 3D space, as well as haptic assistance “as needed” was provided by the Haptic Master robotic arm (Moog-FCS, Netherlands) and finger tracking was done by an instrumented glove (CyberGlove, Immersion, USA). The subject improved her Jebsen Test of Hand Function [19] score from 121 sec to 84 sec, and her Wolf Motor Function Test score from 45 sec to 35 sec. The subject also improved in several kinematic measures of the arm and finger motion during the interactions with the VR simulations.

**III. RESULTS**

Fig. 2 shows the contrast for our effect of interest for each of the three testing sessions. Significant activation was noted in bilateral motor cortex during the post-test session (Fig. 2 and Table 1). No significant activation was noted in motor or premotor areas in the baseline 1 or baseline 2 sessions, even at a liberal threshold. Note that the right cortex activated in the post-test session represents the non-active hemisphere (i.e. corresponding to the hand that was
resting in this condition). Interestingly, the left motor cortex was also recruited in this condition (though weaker) despite the subtracted ellipsoid condition (in which subjects also moved their hand). Thus, the contralateral (mirrored) visual feedback may have had a facilitory effect bilaterally.

IV. DISCUSSION

Our preliminary data demonstrate that time-locking movement of the unaffected hand with high-fidelity movement of the opposite virtual hand that corresponds to the affected side is associated with activation in the ipsilesional, and to a lesser extent the contralesional, motor cortex. This effect was evident only after intense training of the hand and arm on a set of different tasks in a virtual reality environment. Our data suggest that training in virtual reality may bolster remapping in the ipsilesional motor cortex. Moreover, our data may provide a physiological explanation for the benefits reported in several small-scale studies that investigated the efficacy of mirror visual feedback therapy for recovery of hand and arm function in patients with stroke [20,21].

The activation noted in the ipsilesional motor cortex is unlikely to result from uninstructed motion of the affected hand since inspection of hand movement (from the glove data) revealed that the subject complied with the task. Also, our findings are unlikely to result from familiarity with the virtual environment since no effects were noted at the second baseline session. Others have reported that intentional observation of actions can facilitate the magnitude of MEPs and influence corticocortical interactions in the motor and premotor areas [14,22–25]. Further, it is known from retrograde tracer studies that rich intra-hemispheric cortico-cortical connections link the occipital, parietal, and frontal cortices [26–32] and from single unit studies that a substantial number of neurons in motor, premotor, and parietal areas are modulated by visual information [33–36]. Findings of our study are in line with this data and suggest that visual feedback may modulate the motor system without requiring overt movement and that this modulation may be bolstered by (a) training in virtual reality and (b) time-locking the visual feedback with interhemispheric transfer of motor commands. If these findings hold for other patients who are in the chronic phase of stroke, then it will be important to test this principle in the acute phase, when paresis and the potential for neural remapping are greatest.

Acknowledgments

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References


Fig. 1.
Top: The virtual environment used in the current paradigm. We extracted the essential component common to all of our virtual environments, the virtual hands, over a plane background. Bottom: picture of subject’s hands wearing 5DT data gloves that actuated motion of the virtual hand models.
A chronic stroke patient performed a finger sequence with the less affected RIGHT hand. The panels show the activations that were significantly greater when viewing the corresponding finger motion of the LEFT virtual hand (i.e. activation related to ‘mirror’ viewing) than when viewing moving ellipsoids. The right panel shows that after two weeks of intensive training, viewing the LEFT virtual hand while moving the RIGHT hand led to significantly greater bilateral activation of the primary motor cortex, especially IPSILATERAL to the moving hand (i.e. contralateral to the observed virtual hand).
TABLE I

REGIONS IN MNI SPACE SHOWING SIGNIFICANT ACTIVATION FOR THE REPORTED CONTRASTS.

<table>
<thead>
<tr>
<th>Region</th>
<th>X, Y, Z</th>
<th>K</th>
<th>T</th>
<th>P</th>
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<tr>
<td>Right motor cortex</td>
<td>36, −30, 66</td>
<td>194</td>
<td>2.57</td>
<td>0.005</td>
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<tr>
<td>Left motor cortex</td>
<td>−30, −22, 68</td>
<td>50</td>
<td>1.9</td>
<td>0.029</td>
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